

Synthesis and pharmacological activity of a novel water-soluble hepatocyte-specific polymeric prodrug of prostaglandin E₁ using lactosylated poly(L-glutamic hydrazide) as a carrier

Ken Akamatsu, Yasuomi Yamasaki, Makiya Nishikawa, Yoshinobu Takakura,
Mitsuru Hashida*

Department of Drug Delivery Research, Graduate School of Pharmaceutical Sciences, Kyoto University, Sakyo-ku, Kyoto 606-8501, Japan

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Abstract

A novel polymeric prodrug of prostaglandin E₁ (PGE₁) was synthesized using lactosylated poly(L-glutamic hydrazide) (Lac-NH-PLGA) as a targetable carrier to hepatocytes. Poly(L-glutamic hydrazide) (PLGA-HZ) was prepared by reacting poly(γ -benzyl-L-glutamate) with hydrazine monohydrate, followed by coupling with lactose via a hydrazone linkage. Then the lactosylated PLGA-HZ was reduced by sodium cyanoborohydride (NaBH₃CN) in order to make the linkage irreversible (Lac-NH-PLGA). Finally, PGE₁ was bound to hydrazide moieties remaining in Lac-NH-PLGA without any condensing agent under weakly acidic conditions (pH 5) where PGE₁ would be chemically most stable at room temperature (PGE₁ conjugate). The PGE₁ conjugate prepared was sufficiently water-soluble in spite of the hydrophobic nature of its backbone (-NH-CH-CO-) and PGE₁ itself. After intravenous injection in mice, the [¹¹¹In]PGE₁ conjugate rapidly accumulated in the liver, whereas [¹¹¹In]PLGA-HZ did not, suggesting the involvement of a galactose-specific mechanism in the uptake of the [¹¹¹In]PGE₁ conjugate. Fractionation of liver cells revealed that the [¹¹¹In]PGE₁ conjugate was preferentially taken up by liver parenchymal cells. The pharmacological activity was examined in mice with fulminant hepatitis induced by intraperitoneal injection of carbon tetrachloride. Intravenous injection of the PGE₁ conjugate at a dose of 1 mg (0.065 mg PGE₁)/kg effectively inhibited the increase in plasma glutamic pyruvic transaminase (GPT) activity compared with that of free PGE₁ at a dose of 0.065 or 0.65 mg/kg. These results suggest that the PGE₁ conjugate is an excellent prodrug for the treatment of fulminant hepatitis. © 2001 Elsevier Science Inc. All rights reserved.

Keywords: Prostaglandin E₁; Hepatitis; Hepatocyte-specific drug delivery; Lactose; Poly(L-glutamic hydrazide); Cytoprotection

1. Introduction

PGE₁ is well known to have cytoprotective activity and, therefore, it has been reported to be quite effective in fulminant hepatitis [1–5]. However, repetitive or persistent administration of PGE₁ is required for the treatment of hepatitis due to its low hydrophilicity and poor physiological stability [6,7]. Thus, the development of a suitable

delivery system that achieves hepatic targeting of pharmacologically active PGE₁ would be very useful clinically.

Recently, several pharmaceutical approaches to the treatment of hepatitis, using PGE₁, have been investigated. The α -cyclodextrin–PGE₁ complex has also been used for this purpose, and it showed potential in rats in preventing acute hepatitis produced by dimethylnitrosamine, carbon tetrachloride (CCl₄), or D-galactosamine [8,9]. However, as mentioned above, persistent administration is required. Fortunately, we have been able to achieve sugar receptor-mediated selective targeting of various pharmaceutical agents to the liver [10–18]. We have now developed some liver-targeted PGE₁ prodrugs that have potential anti-hepatitis activity even after a single intravenous administration [19–21]. In a recent approach in the series described in this study, galactosylated PLGA-HZ was developed as a drug carrier [20,21]. This carrier macromolecule possesses both

* Corresponding author. Tel.: +81-75-753-4525; fax: +81-75-753-4575

E-mail address: hashidam@pharm.kyoto-u.ac.jp (M. Hashida).

Abbreviations: PGE₁, prostaglandin E₁; PLGA-HZ, poly(L-glutamic hydrazide); Lac-NH-PLGA, lactosylated poly(L-glutamic hydrazide); PGE₁ conjugate, prostaglandin E₁ prodrug using Lac-NH-PLGA as a carrier; DTPA anhydride, diethylenetriamine-N,N,N',N'',N'''-pentaacetic dianhydride; GPT, glutamic pyruvic transaminase; AUC, area under the plasma concentration–time curve; ROS, reactive oxygen species; and EP receptor, receptor for prostaglandins expressed on a plasma membrane.

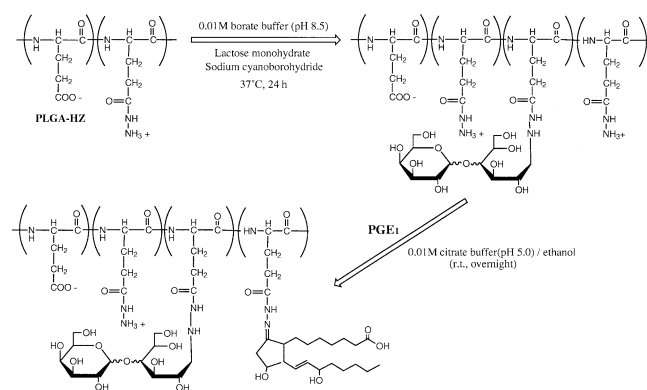


Fig. 1. Synthetic process of a novel polymeric prodrug of PGE₁

hepatocyte-targeting capabilities, i.e. numerous galactose molecules and hydrazine residues for the covalent binding of PGE₁. The PGE₁ polymeric conjugate using this carrier exhibited an excellent hepatitis-inhibiting effect even after bolus administration. Nevertheless, this conjugate tended to gradually aggregate, probably due to the reduced hydrophilicity of the conjugate following PGE₁ binding or intramolecular electric interactions. To combat these disadvantages, a new carrier with lactose instead of galactose residues was synthesized as a hepatocyte-targeting device. The biodistribution in mice of the PGE₁ conjugate using the Lac-NH-PLGA was determined, and then the pharmacological activity of the PGE₁ conjugate was examined in mice with carbon tetrachloride-induced fulminant hepatitis.

2. Materials and methods

2.1. Chemicals and animals

Poly(γ -benzyl-L-glutamate) with an average molecular weight of approximately 17,300 (degree of polymerization: 79) was purchased from the Sigma Chemical Co. Lactose monohydrate and hydrazine monohydrate were obtained from Wako Pure Chemicals. Sodium cyanoborohydride (NaBH₃CN) was obtained from the Aldrich Chemical Co. DTPA anhydride was obtained from Dojindo Laboratory. PGE₁ was obtained commercially and used without further purification. Male ddY mice (25–30 g) were obtained from the Shimizu Agricultural Cooperative Association for Laboratory Animals.

2.2. Synthesis of PGE

For the synthesis of the PGE₁ conjugate (Fig. 1), poly(γ -benzyl-L-glutamate) was prepared by the method of Hurwitz *et al.* [22]. Five hundred milligrams of poly(γ -benzyl-L-glutamate) was suspended in 10 mL of hydrazine monohydrate with stirring at room temperature for 3 hr to obtain a homogeneous solution. The reaction mixture obtained was transferred into dialysis tubing (3 kDa cut-off) followed by

the addition of 40 mL of water (if a gel formed, aqueous HCl was added) and then dialyzed thoroughly against distilled water. The dialysate was concentrated by ultrafiltration (10 kDa cut-off) and lyophilized to obtain PLGA-HZ. The hydrazide group content of PLGA-HZ was measured photometrically using β -naphthoquinone-4-sulfonate [23].

PLGA-HZ (50 mg) was dissolved in 1 mL of 5 N NaOH solution and neutralized by adding 5 N HCl solution. Three milliliters of 0.1 M borate buffered solution (pH 8.5) was added to the PLGA-HZ solution to bring the pH to 8–9. Lactose monohydrate (143 mg) and sodium cyanoborohydride (50 mg) were added to the PLGA-HZ solution above and stirred overnight at 37°. The reaction mixture was transferred into dialysis tubing (3 kDa cut-off) and dialyzed thoroughly against distilled water. The dialysate obtained was concentrated by ultrafiltration (10 kDa cut-off) and then lyophilized to obtain reduced Lac-NH-PLGA. The number of lactose residues in the Lac-NH-PLGA was determined by the anthrone-sulfuric acid method and found to be 22 mol/mol of conjugate.

For binding PGE₁ to Lac-NH-PLGA, initially, PGE₁ (2.8 mg) was dissolved in 0.5 mL ethanol (or containing a trace amount of [³H]PGE₁). The PGE₁ ethanolic solution was added slowly in drop-wise fashion to Lac-NH-PLGA (23 mg) dissolved in 5 mL of 0.01 M acetate-buffered solution (pH 5.0) with stirring overnight at room temperature. Purification of the reaction mixture was carried out as described above. The resulting product was water-soluble. The PGE₁ content of the conjugate was determined by counting the radioactivity of [³H]PGE₁ and found to be 4 mol/mol of conjugate.

2.3. Biodistribution experiment

To study the disposition of PLGA-HZ and the PGE₁ conjugate, they were radiolabeled with ¹¹¹In using DTPA anhydride as described previously [12]. Each radiolabeled derivative was purified by gel-filtration chromatography using a Sephadex G-25 column [1.5 × 5.0 cm, 0.1 M acetate buffer (pH 6.0)] and found to have a specific activity of approximately 37 MBq. Mice received a 1 or 10 mg/kg dose of [¹¹¹In]PLGA-HZ and [¹¹¹In]PGE₁ conjugate in saline by tail vein injection and were housed in metabolic cages to allow urine collection. At appropriate intervals after injection, blood was collected from the vena cava under ether anesthesia, and plasma was obtained by centrifugation. The heart, lungs, liver, spleen, and kidneys were excised, rinsed with saline, and weighed, and their radioactivity was determined. The amount of radioactivity in the urine was determined by collecting both the urine excreted and that remaining in the bladder. In addition, the distribution of these macromolecules in liver parenchymal and nonparenchymal cells was determined by separating these cells using collagenase after intravenous injection as previously reported [18]. ¹¹¹In radioactivity was counted in a well-type NaI scintillation counter (ARC-500, Aloka). Also, the ³H radio-

activity was measured in a standard liquid scintillation counter (LSC-5000, Beckman), after dissolution in Soluene-350 (Packard) and addition of a scintillation medium, Clear-sol I (Nakalai Tesque). Radioactivity originating from the plasma in each tissue sample was corrected using the distribution data for [^{111}In]BSA at 10 min after intravenous injection [13], assuming that [^{111}In]BSA is not taken up by tissues during the 10-min period.

2.4. Pharmacokinetic analysis

Tissue distribution patterns of [^{111}In]PLGA derivatives were evaluated from the organ uptake clearance (CL_{org}) according to the method previously reported [24]. In the early period after injection, the efflux of ^{111}In radioactivity from organs is assumed to be negligible, since the degradation products of ^{111}In -labeled ligands using DTPA cannot cross biological membranes easily [25,26]. Using the assumption described above, the CL_{org} was calculated by dividing the amount of radioactivity in an organ at 10 min by the AUC up to the same time point. The AUC and total-body clearance (CL_{total}) were calculated by fitting an equation derived from a linear one- or two-compartment open model to the plasma concentration data of the derivatives using the nonlinear least-squares program MULTI [27].

2.5. In vivo pharmacological activity of the PGE_1 conjugate

The pharmacological activity of the PGE_1 conjugate was evaluated by measuring the GPT activity in the plasma of mice with fulminant hepatitis induced by CCl_4 . Mice received an intraperitoneal injection of CCl_4 (2% solution in sesame oil) at a dose of 10 mL/kg. Immediately after CCl_4 administration, the PGE_1 conjugate (1 or 10 mg/kg) or free PGE_1 (0.065 or 0.65 mg/kg) solution was injected intravenously into the tail vein. The mice were then starved for 18 hr after CCl_4 administration, blood was collected from the vena cava under ether anesthesia, and plasma was obtained by centrifugation at 2000 g for 5 min at 4°. The GPT activity in the plasma sample was determined by the UV-rate method [28].

3. Results

3.1. Plasma clearance and tissue distribution of ^{111}In -labeled PLGA-HZ and PGE_1 conjugate

Figure 2 shows the time courses of the plasma concentration and tissue accumulation of PLGA-HZ and PGE_1 conjugate. The PGE_1 conjugate was eliminated rapidly from the plasma and accumulated mainly in the liver [up to 60% of a dose of 1 mg/kg within 10 min] by recognition of the galactose moieties by asialoglycoprotein receptors [10–18], whereas at a dose of 10 mg/kg up to only 35% of the dose

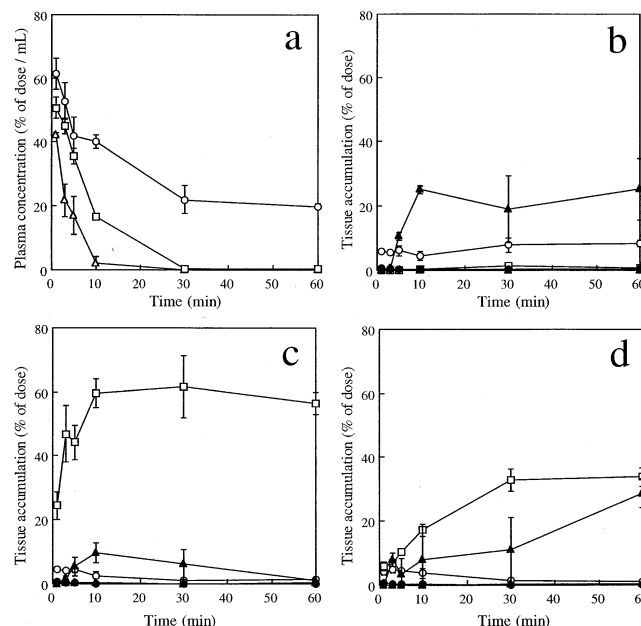


Fig. 2. Plasma concentration and tissue accumulation time courses of [^{111}In]PLGA-HZ and the [^{111}In]PGE $_1$ conjugate after intravenous injection in mice. Results are expressed as the means \pm SD of three mice. (Panel a) plasma concentration–time courses of [^{111}In]PLGA-HZ at a dose of 1 mg/kg (\circ), and the [^{111}In]PGE $_1$ conjugate at a dose of 1 mg/kg (0.065 mg of equivalent PGE $_1$ /kg) (Δ) or 10 mg/kg (0.65 mg of equivalent PGE $_1$ /kg) (\square). (Panels b–d) Tissue accumulation–time courses of (b) [^{111}In]PLGA-HZ at a dose of 1 mg/kg, (c) [^{111}In]PGE $_1$ conjugate at a dose of 1 mg/kg and (d) [^{111}In]PGE $_1$ conjugate at a dose of 10 mg/kg [kidney, (\circ); spleen, (Δ), liver, (\square); lung, (\bullet); and urine, (\blacktriangle)].

accumulated in the liver following saturation of the sugar receptor (Fig. 2, panels a and c). At both doses, renal excretion seemed to be another elimination pathway for the conjugate, since a slight accumulation in the kidneys at the early phase and subsequent urinary excretion were observed. There was no significant accumulation of the PGE_1 conjugate in other tissues including the spleen and lungs. In contrast to the PGE_1 conjugate, PLGA-HZ without lactose (galactose) units hardly accumulated in the liver, but was excreted in the urine (Fig. 2, panels a and b). Also, the extremely small AUC and large hepatic clearance values of the PGE_1 conjugate reflected these results (Table 1).

3.2. Cellular distribution of ^{111}In -labeled PLGA-HZ and PGE_1 conjugate in liver

The hepatic cellular localization study of the carrier (Fig. 3) shows that it was selectively taken up by parenchymal cells. These data suggest that, using the polymeric drug carrier, potential PGE_1 should be successfully targeted to liver parenchymal cells without any metabolism following intravenous administration by this delivery system.

3.3. Therapeutic activity of the PGE_1 conjugate in mice with acute hepatitis

Figure 4 shows the GPT levels in the plasma of normal mice and mice with hepatitis induced by CCl_4 and then

Table 1

AUC and clearances for [^{111}In]PLGA-HZ and [^{111}In]PGE₁ conjugate after intravenous injection in mice

Compounds ^a	Dose (mg/kg)	AUC ^{b,c} (% of dose · hr/mL)	Clearance ($\mu\text{L/hr}$) ^c					
			CL _{total}	CL _{liver}	CL _{kidney}	CL _{urine}	CL _{spleen}	CL _{lung}
[^{111}In]PLGA-HZ	1	250	410	0.80	18.0	110	0.13	1.6
[^{111}In]PGE ₁ conjugate	1	8.7	30,000	19,000	730	3100	70	35
[^{111}In]PGE ₁ conjugate	10	3.4	12,000	2800	2000	3200	8.0	130

^a PGE₁ conjugate contains 0.065 mg PGE₁/mg of the conjugate.^b AUC: are as under the plasma concentration-time curve.^c AUC and clearance data are expressed as average values of three mice for 10 min after intravenous injection.

treated with PGE₁ or its polymeric conjugate. It can be seen that the PGE₁ polymeric conjugate strongly inhibited the increase in GPT concentration in the plasma; this inhibition was more effective than that of a bolus administration of free PGE₁.

4. Discussion

The Lac-NH-PLGA prepared in this study was more water-soluble than the galactosylated PLGA previously reported [21]. This is due to the increased number of OH moieties in the carrier due to the glucose units in lactose. It is generally important to increase the hydrophilicity of the carrier because most drugs, as well as PGE₁, have a relatively similar hydrophobicity. In addition, lactose and PGE₁ are not only readily bound to PLGA-HZ, but also the chemical structure of PGE₁ remains unchanged during the reaction (Fig. 1) because PGE₁ is chemically most stable around pH 4–5 [6]. Therefore, this lactosylated carrier will be

applicable to any drugs that are stable under weakly acidic conditions having an aliphatic aldehyde or carbonyl moiety in their chemical structure.

The lactosylated (galactosylated) prodrug was targeted to the liver via the recognition of asialoglycoprotein receptors on the plasma membrane of the parenchymal cell [10–18]. However, a high concentration of the galactose should lead to saturation of the receptors. In the pharmacological activity experiment, a similar therapeutic effect was observed at lower (1 mg/kg) and higher (10 mg/mL) doses of the lactosylated PGE₁ conjugate (Fig. 4). Receptor saturation may be responsible for these results. If this were the case, a similar amount of the PGE₁ conjugate would be internalized in the liver parenchymal cells at both concentrations, which would result in similar pharmacological activities. Furthermore, the biodegradation rate of the carrier or the release

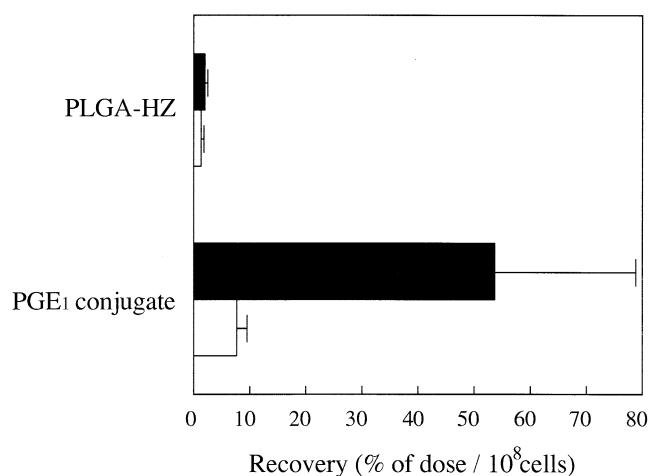


Fig. 3. Hepatic cellular localization of radioactivity after intravenous injection of [^{111}In]PLGA-HZ and the [^{111}In]PGE₁ conjugate in mice at a dose of 1 mg/kg. The unit of recovery was expressed as percent of dose per 10^8 cells, considering that the numbers of hepatic parenchymal cells (■) and nonparenchymal cells (□) in a mouse were estimated to be 1.25×10^6 and 0.65×10^6 cells/g liver, respectively [29]. Results are expressed as the means \pm SD of three mice.

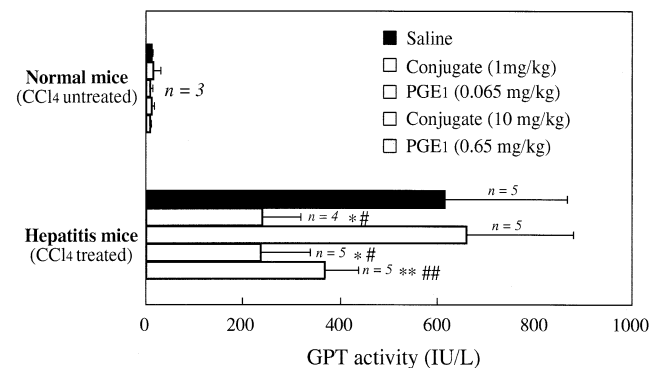


Fig. 4. GPT levels in the plasma of normal or hepatitis mice treated by PGE₁ or the PGE₁ conjugate (4 mol PGE₁/mol conjugate). Statistically significant differences were determined based on ANOVA (Student-Newman-Keuls multiple comparisons test). Key: (*, **) compared with saline-treated mice (*: $P < 0.01$, **: $P < 0.05$), and (#, ##) compared with PGE₁-treated mice (#: $P < 0.01$; ##: $P < 0.05$). Results are expressed as the means \pm SD of at least three mice. Hepatitis was induced in mice by intraperitoneal injection of CCl₄ (2% solution in sesame oil) at a dose of 10 mL/kg. In this experiment, four kinds of drug solution were prepared: saline, 0.9% NaCl; PGE₁, 0.2 mg/mL of polyethyleneglycol solution; PGE₁ conjugate, 0.1 or 1 mg/mL of aqueous solution. Each solution of PGE₁ conjugate was injected intravenously into the tail vein at a dose of 1 or 10 mg/kg, respectively. GPT activity in the plasma samples, obtained from the vena cava, was assessed 18 hr after collection and was measured by the UV-rate method [28]. The order of the symbols in the key represents the order of the bars in the figure.

rate of the PGE₁ molecule from the carrier may, in part, affect the pharmacological efficacy. At a higher dose, these rates should be also reduced.

Our method for the estimation of the therapeutic activity may prove clinically impractical: CCl₄-induced fulminant or acute hepatitis is unlikely to occur in humans, and is almost irreversible, and the PGE₁ conjugate was administered immediately after CCl₄ injection. However, if the PGE₁ conjugate is injected several hours after CCl₄ administration, it should be no more effective. In addition, free PGE₁ would not be released from the carrier until the carrier molecules binding PGE₁ are digested in the hepatic parenchymal cells. Taking the delay time into account, clinically the drug should be administered as soon as possible after poisoning.

The cytoprotective effects of PGE₁, PGE₂, and their chemically stable analogs (PGEs) have been studied using mainly hepatocytes, gastrointestinal cells, spermatocytes, and Chinese hamster ovary (CHO) K1 cells *in vivo* or *in vitro* in terms of a variety of stimulating factors, e.g. ethanol [30–32], nonsteroidal anti-inflammatory drugs (NSAIDs) [33], ROS [34,35], deoxycholate [36], actinomycin C [37], D-galactosamine [9], and ionizing radiation [38] as well as CCl₄. Thus, PGEs generally defend cells against cell death, i.e. apoptosis or necrosis, as an endpoint. In the case of agents that cause damage to DNA, such as actinomycin C, ROS, or ionizing radiation, the cytoprotective effects of PGEs may be due to their ability to promote DNA repair, which could be triggered by the binding of EP₂ receptor subtypes expressed on the plasma membrane to the ligand [38], while their protective effects against agents that do not cause damage to DNA, e.g. ethanol, are thought to involve the EP₁ receptor subtype [30]. The effect against other stimulators, such as CCl₄, remains unknown. Thus, the cytoprotective mechanisms of PGEs are complex and unclear at present. Nevertheless, we have designed the novel polymeric prodrug of PGE₁ for the treatment of hepatitis in order to increase the overall hepatic uptake of active PGE₁, using sugar receptor-mediated internalization into hepatocytes.

The present study has demonstrated that the novel PGE₁ polymeric prodrug not only is delivered into hepatocytes effectively but also exhibits greater cytoprotective activity than free PGE₁. Although the detailed mechanism for its pharmacological activity is unclear, we believe that free PGE₁ released from the conjugate is responsible for its effect. A previous study [21] has confirmed that PGE₁ (or its derivatives) is released from the carrier, galactosylated PLGA-HZ, in liver homogenate but not in phosphate-buffered saline (pH 7.4 at 37°), suggesting that certain enzymes in the liver may be needed for the release of PGE₁. It is unlikely that PGE₁ conjugated with the polymeric carrier is active because the interacting site in the PGE₁ molecule for the EP receptor is blocked by its hydrazone linkage (Fig. 1). PGE₁ released from the carrier in hepatocytes may bind to EP receptors on the cell or neighboring hepatocytes passing

through the plasma. However, in accordance with a few reports [30,38], interaction of PGE₁ with EP receptors should play an important role in its pharmacological activity, although no other sites of action for PGE₁ have been reported. Hence, the advantage of the delivery system for PGE₁ is that it allows active PGE₁ molecules to be released gradually within and in the vicinity of hepatocytes. This characteristic avoids down-regulation of the EP receptors induced by bolus administration.

Hepatic injury produced by CCl₄ can be induced not only by direct plasma membrane oxidation in the parenchymal cells but also by cytotoxic cytokines and tumor necrosis factor- α produced from activated Kupffer cells. Kayano *et al.* [39] have demonstrated that PGE₁ can suppress the activation of Kupffer cells. Although most PGE₁ molecules would be internalized into liver parenchymal cells using the polymeric carrier, part of the PGE₁ passing through the plasma membrane might have an effect on Kupffer cells.

In the CCl₄-induced fulminant hepatitis model, bolus injection of 1 mg/kg (0.065 mg PGE₁/kg) of the PGE₁ conjugate immediately after CCl₄ administration was more cytoprotective than that of 0.65 mg/kg of free PGE₁ (Fig. 4), suggesting that the conjugate was 10-fold more effective than free PGE₁ in the model. This result implies that the chemical structure of the drug or its pharmacological activity has been maintained before internalization into the hepatocytes following intravenous administration, while free PGE₁ should be metabolized very fast, particularly in the lungs [40]. Consequently, the pharmacological efficiency of PGE₁ as an anti-hepatitis drug was improved markedly by using the hepatocyte-specific carrier system. To assess the practical relevance of the conjugate, further studies should be carried out based on hepatitis models other than the CCl₄-induced model.

In conclusion, we have developed a novel water-soluble polymeric prodrug of PGE₁ targetable to hepatocytes. The PGE₁ polymeric prodrug may be useful as a therapeutic agent for inflammatory liver diseases including hepatitis. The agent could also be a powerful tool for clarifying the mechanism of the therapeutic effect of PGE₁ against hepatitis induced by CCl₄.

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